



## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

<p>(51) International Patent Classification<sup>6</sup> : <b>A61K 31/435</b></p>	<p><b>A2</b></p>	<p>(11) International Publication Number: <b>WO 98/10762</b> (43) International Publication Date: 19 March 1998 (19.03.98)</p>
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<p>(54) Title: CONTROLLED RELEASE DOSAGE FORM OF [R-(Z)]-ALPHA-(METHOXYIMINO)-ALPHA-(1-AZABICYCLO[2.2.2]OCT-3-YL)ACETONITRILE MONOHYDROCHLORIDE</p>		
<p>(57) Abstract</p> <p>A controlled release formulation of an acetonitrile compound and its use in the treatment and/or prophylaxis of certain disorders.</p>		

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**CONTROLLED RELEASE DOSAGE FORM OF [R-(Z)]-ALPHA-(METHOXYIMINO)-ALPHA-(1-AZABICYCLO[2.2.2]OCT-3-YL)ACETONITRILE MONOHYDROCHLORIDE**

The present invention relates to a novel formulation, and to its use in the treatment and/or prophylaxis of certain disorders.

5 [R-(Z)]- $\alpha$ -(methoxyimino)- $\alpha$ -(1-azabicyclo [2.2.2]oct-3-yl)acetonitrile monohydrochloride (compound X) and methods for its preparation are disclosed in EP-A-0392803, WO95/31456 and WO93/17018. The compound enhances acetylcholine function via an action at muscarinic receptors within the central nervous system, and is therefore of potential use in the treatment and/or prophylaxis of dementia in mammals.

10 WO96/12486 discloses the use of compound X in the manufacture of a medicament for enhancing amyloid precursor protein processing along a non-amyloidogenic pathway in patients suffering from, or at risk of developing, Alzheimer's disease.

15 Fast-release swallow tablet and oral solution formulations of compound X both result in rapid absorption of the compound into the circulation, and require twice a day dosing for optimal efficacy.

20 It has now been surprisingly found that it is possible to formulate compound X, which has very high water solubility and is active at extremely low doses, in such a way that release is controlled to take place over a period of hours. Such a formulation would require dosing only once a day: this is likely to improve compliance in a patient population characterised by poor memory; it may also reduce side-effects in case of accidental overdosing.

25 Accordingly, the present invention provides a controlled release oral dosage form containing compound X, its parent free base or any other pharmaceutically acceptable salt thereof.

By controlled release is meant any formulation technique wherein release of the active substance from the dosage form is modified to occur at a slower rate than that from an immediate release product, such as a conventional swallow tablet or capsule.

30 Controlled release includes delayed release wherein release of the active substance from the dosage form is modified to occur at a later time than that from a conventional immediate release product. The subsequent release of active substance from a delayed release formulation may also be controlled to occur at a slower rate.

Examples of controlled release formulations which are suitable for incorporating compound X are described in:

35 Sustained Release Medications, Chemical Technology Review No. 177. Ed. J.C. Johnson. Noyes Data Corporation 1980.

Controlled Drug Delivery, Fundamentals and Applications, 2nd Edition. Eds. J.R. Robinson, V.H.L. Lee. Marcel Dekker Inc. New York 1987.

Such controlled release formulations are preferably formulated in a manner such that release of compound X is effected throughout the gastro-intestinal tract, and takes place predominantly over the first eight to twelve hours following ingestion.

Preferred formulations include wax matrices, swellable and/or gellable polymer or hydrogel matrices, tablets coated with release controlling polymers or waxes, and pellets, granules or beads comprising matrices or coated with release controlling polymers or waxes and then formulated as capsules, compressed tablets or suspensions.

Suitable waxes for matrix formation or release controlling coating include non-ionic beeswax derivatives such as Gelucire 62/05, 50/02 or 50/13 (Gattefosse), glyceryl behenate, other fatty acid mono-, di- or tri-esters of glycerol such as Precirol ATO5 (Gattefosse), microcrystalline wax, hydrogenated castor oil or hydrogenated vegetable oil, long-chain aliphatic alcohols such as stearyl alcohol and carnuba wax.

Suitable materials for the formation of hydrogel matrices or swellable and/or gellable polymer matrices may be selected from alkyl celluloses, hydroxyalkylcelluloses, polyvinyl alcohol, polymethacrylates, polymethylmethacrylates, methacrylate/divinylbenzene copolymers, carboxymethylamide, polyoxyalkylene glycols, polyvinyl pyrrolidone and carboxymethyl cellulose. The swellable polymeric material in particular may be selected from crosslinked sodium carboxymethylcellulose, crosslinked hydroxypropylcellulose, high molecular weight polyhydroxypropylmethylcellulose, carboxymethylamide, potassium methacrylate/divinylbenzene copolymer, polymethylmethacrylate, crosslinked polyvinylpyrrolidone and high molecular weight polyvinyl alcohol. The gellable polymeric material in particular may be selected from methylcellulose, carboxymethylcellulose, low-molecular weight hydroxypropylmethylcellulose, low-molecular weight polyvinylalcohols, polyoxyethyleneglycols and non-cross-linked polyvinylpyrrolidone. The swellable and gellable polymeric material in particular may be selected from medium-viscosity hydroxypropylmethylcellulose and medium-viscosity polyvinylalcohols.

Release controlling polymers include hydrogel polymers such as those listed above, hydrophobic polymers and enteric, or pH dependent, polymers.

Suitable materials for the formation of hydrophobic release controlling polymer coatings include alkyl celluloses, which may be used in the form of latex suspensions such as Surelease (Colorcon) or Aquacoat (FMC), and methacrylic acid derivatives, which may be used in the form of latex suspensions such as Eudragit RS, RL and NE (Rohm).

Suitable materials for the formation of enteric or pH dependent polymer coatings include methacrylic acid derivatives, which may be used in the form of latex suspensions such as Eudragit L and S (Rohm).

Seal coats, film layers used to separate the various functional layers of the formulation or to provide a final layer to the outside of the formulation, contain suitable materials for film forming such as alkylcelluloses, which may be used in the form of latex suspensions such as Surelease (Colorcon) or Aquacoat (FMC), and hydroxyalkylcelluloses such as hydroxypropylmethylcellulose (for example Opadry (Colorcon)).

The formulation may also include plasticisers such as triethyl citrate, dibutyl sebacate or medium chain triglycerides in the release controlling polymer layer.

Pellet-forming materials include suitable grades of microcrystalline cellulose such as Avicel PH101 (FMC).

Granules may be formed from any of the commonly used pharmaceutical fillers or diluents such as lactose, lactose monohydrate, mannitol, microcrystalline cellulose, dicalcium phosphate or starch.

Beads may be formed by layering or spraying on non-pareil seeds.

Other suitable ingredients in controlled-release dosage forms include polyethylene glycol and propylene glycol and these, as well as the pharmaceutical fillers, may be used to modify the release rate by inclusion in matrices, pellets, granules or beads.

The formulation may also include hydrophobic excipients that retard the release from the formulation such as ethylcellulose, talc, colloidal silicon dioxide or glyceryl monostearate and/or one or more binders such as hydroxypropylmethylcellulose, microcrystalline cellulose or polyvinylpyrrolidone.

Wetting agents such as sodium lauryl sulphate, lubricants such as magnesium stearate and glidants such as colloidal silica may also be included.

A particularly preferred formulation comprises drug-layered beads coated with a release controlling polymer either alone or in combination with drug-layered beads not coated with a release controlling polymer (immediate release beads). In the drug layering process onto non-pareil beads, appropriate size non-pareil sugar beads may be layered with a solution or dispersion containing the active substance, inert excipients, and/or retardants such as ethylcellulose, talc, colloidal silicon dioxide or glyceryl monostearate and/or one or more binders such as hydroxypropylmethylcellulose or polyvinylpyrrolidone. The layering of the active substance may be accomplished at a predetermined rate and temperature using either a coating pan or a fluid bed drier. The layered beads may be seal coated with a suitable film forming polymer such as hydroxypropylmethylcellulose (e.g. Opadry) or Eudragit® L30D-55 (a methacrylic acid copolymer) and then may be coated with one or more suitable release controlling polymers preferably selected from from alkyl celluloses, hydroxyalkylcelluloses, sodium carboxymethyl cellulose and methacrylic acid derivatives, such as ethylcellulose, Eudragit® RS, Eudragit® RL or Methocel E4M, to produce beads that release compound

X over an eight to twelve hour period and/or release compound X in one or more pulses. Seal coated beads may be used for an immediate release dose. The controlled release or a mixture of controlled release and immediate release beads may then be filled into an appropriate size capsule or compressed with inert excipients into tablets of appropriate physical parameters such as shape, size, hardness and disintegration. The polymer(s), release controlling plus any seal coat polymer(s), preferably make up 10 to 30% by weight of the total dosage form. Plasticizer is normally present and may make up at least 2% by weight. Binder(s) and retardant(s) typically make up to 3-10% by weight.

Another particularly preferred formulation comprises a swellable and/or gellable polymer matrix tablet. The polymer matrix is preferably a hydrogel polymer selected from alkyl celluloses such as methylcellulose, hydroxyalkylcelluloses such as hydroxypropylcellulose and hydroxypropylmethylcellulose, polyvinyl alcohol, polymethacrylates, cross-linked polyvinylpyrrolidone and sodium carboxymethyl cellulose. The polymers typically make up 10 to 50% by weight of the tablet. The matrix tablet can be sealed with a hydrophobic release controlling polymer coating such as ethylcellulose (Surelease (Colorcon)) to retard the hydration of the hydrogel matrix in the tablet. The hydrophobic coating polymer typically make up 4 to 10% by weight of the tablet.

Such matrix tablet formulations can be prepared by either direct compression or wet granulation processes. Coating may be accomplished using a coating pan.

Other preferred formulations are described in US Patent No. 5,422,123.

Thus, a particular aspect of the invention provides a system for the controlled release of an active substance which is compound X, its parent free base or any other pharmaceutically acceptable salt thereof, comprising (a) a deposit-core comprising an effective amount of the active substance and having defined geometric form, and (b) a support-platform applied to said deposit-core, wherein said deposit-core contains at least the active substance, and at least one member selected from the group consisting of (1) a polymeric material which swells on contact with water or aqueous liquids and a gellable polymeric material wherein the ratio of the said swellable polymeric material to said gellable polymeric material is in the range 1:9 to 9:1, and (2) a single polymeric material having both swelling and gelling properties, and wherein the support-platform is an elastic support, applied to said deposit-core so that it partially covers the surface of the deposit-core and follows changes due to hydration of the deposit-core and is slowly soluble and/or slowly gellable in aqueous fluids.

The swellable polymeric material in (1) may be selected from crosslinked sodium carboxymethylcellulose, crosslinked hydroxypropylcellulose, high molecular weight polyhydroxypropyl-methylcellulose, carboxy-methyl starch, potassium

methacrylate/divinylbenzene copolymer, crosslinked polyvinylpyrrolidone and polyvinyl alcohol. The gellable polymeric material in (1) may be selected from methylcellulose and non-cross-linked polyvinylpyrrolidone.

The support-platform may comprise; polymers such as  
5 polyhydroxypropylmethylcellulose, polyvinyl alcohol, polyacrylate, polymethacrylate, polyhydroxypropyl cellulose and polysodium carboxymethylcellulose; plasticizers such as polyoxyethylene glycols, castor oil, hydrogenated castor oil, ethyl phthalate, butyl phthalate, natural glycerides, synthetic glycerides and semisynthetic glycerides; binders  
10 such as polyvinylpyrrolidone, methylcellulose, ethyl cellulose gum arabic and alginic acid; hydrophilic agents such as mannitol, lactose, starch and colloidal silica; and/or hydrophobic agents such as hydrogenated castor oil, magnesium stearate, a fatty substance, wax, natural glycerides and synthetic glycerides. The polymer(s) typically make up 30 to 90% by weight of the support-platform, for example about 35 to 40%. Plasticizer may make up at least 2% by weight of the support-platform, for example about  
15 15 to 20%. Binder(s), hydrophilic agent(s) and hydrophobic agent(s) typically total up to about 50% by weight of the support-platform, for example about 40 to 50%.

Such formulation may be prepared as generally described in US 5,422,123.

US-A-4 839 177 discloses a further alternative controlled release formulations suitable for use in the present invention.

20 Thus a further aspect of the invention provides a system for the controlled-rate release of compound X, consisting of:  
a) a deposit-core comprising effective amounts of compound X and having defined geometric form,  
b) a support-platform applied to said deposit-core wherein said deposit-core contains,  
25 mixed with the active substance, at least one member selected from the group consisting of a (a) 5-80% by weight of the total weight of deposit-core of a polymeric material having a high degree of swelling on contact with water or aqueous liquids and 90-10% by weight of the total weight of the deposit core of a gellable polymeric material. and (b) a single polymeric material having both swelling and gelling properties, and other  
30 adjuvants able to provide the mixture with suitable characteristics for compression and for intake of water, and wherein said support-platform consists of a polymeric material insoluble in aqueous liquids and partially coating said deposit core.

The swellable polymeric material in (a) may be selected from crosslinked sodium carboxymethylcellulose, crosslinked hydroxypropylcellulose, high molecular weight  
35 polyhydroxypropyl-methylcellulose, carboxy-methylamide, potassium methacrylate/divinylbenzene copolymer, polymethylmethacrylate, crosslinked polyvinylpyrrolidone and high molecular weight polyvinyl alcohol. The gellable polymeric material in (a) may be selected from methylcellulose, carboxymethylcellulose.

low-molecular weight hydroxypropylmethylcellulose, low-molecular weight polyvinylalcohols, polyoxyethyleneglycols and non-cross-linked polyvinylpyrrolidone. The swellable and gellable polymeric material in (b) may be selected from medium-viscosity hydroxypropylmethylcellulose and medium-viscosity polyvinylalcohols. The support platform may comprise insoluble polymeric material selected from acrylates, cellulose, ethylcellulose, cellulose acetate-propionate, polyethylene, methacrylates, acrylic acid copolymers and high-molecular weight polyvinylalcohols.

Such formulation may be prepared as generally described in US 4,839,177.

WO 94/06416 discloses a yet further alternative controlled release formulations suitable for use in the present invention.

Thus a yet further aspect of the invention provides a system for the controlled-rate release of compound X, consisting of a pharmaceutical compressed tablet capable of releasing compound X at different rates, consisting of three layers, wherein

- a first layer contains compound X with immediate or controlled release formulation, composed of rapidly swelling and/or soluble and/or erodible polymeric substances by contact with aqueous fluids, and adjuvants;
- a second layer contains compound X, either equal to or different from those of the first layer, with slow release formulation, composed of swelling and/or gellable and/or erodible polymeric substances by contact with aqueous fluids, and adjuvants;
- a low-permeability barrier-type layer coating said second layer or, alternatively, placed between the first and second layer, consisting of polymeric substances, adjuvants, plasticizing agents and, if necessary, compound X.

The polymeric substances of the first layer may be selected from cross-linked polyvinylpyrrolidone, low- and medium-molecular-weight hydroxypropyl cellulose and hydroxypropyl methylcellulose, cross-linked sodium carboxymethylcellulose, carboxymethyl starch, potassium methacrylate-divinylbenzene copolymer, polyvinyl alcohols, starches, starch derivatives, microcrystalline cellulose and cellulose derivatives,  $\beta$ -cyclodextrin and dextrin derivatives.

The polymeric substances of the second layer may be selected from the group consisting of hydroxypropyl methylcellulose having molecular weight from 1,000 to 4,000,000, hydroxypropyl cellulose having molecular weight from 2,000 to 2,000,000, carboxyvinyl polymers, polyvinyl alcohols, glucans, scleroglucans, mannans, xanthans, alginic acid and derivatives thereof, carboxymethylcellulose and derivatives thereof, poly(methyl vinyl ethers/maleic anhydride), ethylcellulose, methylcellulose, and cellulose derivatives.

The adjuvants of the first and second layers may be selected from the group consisting of starch, pregelled starch, calcium phosphate, mannitol, lactose, saccharose, glucose, sorbitol, microcrystalline cellulose, gelatin, polyvinylpyrrolidone,



methylcellulose, starch solution, ethylcellulose, arabic gum, tragacanth gum, magnesium stearate, stearic acid, colloidal silica, glyceryl monostearate, hydrogenated castor oil, waxes, and mono-, bi-, and trisubstituted glycerides.

5 The polymeric substances of the barrier type layer may be selected from the group consisting of hydroxypropyl methylcellulose having molecular weight from 1,000 to 4,000,000, hydroxypropyl cellulose having molecular weight from 2,000 to 2,000,000, carboxyviny polymers, polyvinyl alcohols, glucans, scleroglucans, mannans, xanthans, carboxymethylcellulose, ethylcellulose, and methylcellulose.

10 The adjuvants of the barrier-type layer may be selected from the group consisting of glyceryl monostearate, semisynthetic glycerides, glyceryl palmitostearate, glyceryl behenate, polyvinylpyrrolidone, gelatine, ethylcellulose, methylcellulose, sodium carboxymethylcellulose, magnesium stearate, stearic acid, sodium stearate, talc, sodium benzoate, boric acid, and colloidal silica.

15 The plasticizing agents of the barrier-type layer may be selected from the group consisting of hydrogenated castor oil, fatty acids, substituted triglycerides and glycerides, polyoxyethylene glycols and derivatives thereof having molecular weight from 400 to 60,000.

Such formulation may be prepared as generally described in WO 94/06416.

The dosage form preferably contains compound X itself.

20 Compound X has active doses around 5-125 microgramme ( $\mu\text{g}$ ) (calculated as free base). It has been found through administration to human patients that efficacy as a cognition enhancer may be obtained at daily doses below 0.01mg/kg more particularly 0.003mg/kg and below, for example 0.0001-0.003mg/kg, such as 0.00035-0.003mg/kg, 0.0007-0.003mg/kg, 0.0001-0.0007mg/kg or 0.00035-0.002mg/kg.

25 Suitable unit doses to achieve such daily doses are 5, 12.5, 25, 50 or 75 $\mu\text{g}$ , administered twice daily or 50 $\mu\text{g}$  or 100 $\mu\text{g}$ , once daily. Such unit doses are calculated on the basis of 50-70kg individuals and as free base.

30 Suitably, the *in vitro* release profile of the dosage form i.e. the amount of compound X released over time will be selected so that it will provide an area under the *in vivo* plasma profile curve that is similar to that obtained following conventional oral administration of a fast release tablet, 5 to 75 $\mu\text{g}$  (calculated as free base) compound X twice a day. Preferably 25-70% is released over 4hours and 70-100% is released over 8 hours.

35 The dosage form of the invention may be used in the treatment and/or prophylaxis of dementia, including Alzheimer's disease, in mammals, and for enhancing amyloid precursor protein processing along a non-amyloidogenic pathway in patients suffering

from, or at risk of developing, Alzheimer's disease. These disorders are herein after referred to as "the Disorders".

The present invention provides a method of treating "the Disorders" by administering an effective amount of a controlled release oral dosage form containing compound X, its parent free base or any other pharmaceutically acceptable salt thereof, to a sufferer in need thereof.

The present invention further provides the use of a controlled release oral dosage form containing compound X, its parent free base or any other pharmaceutically acceptable salt thereof, in the manufacture of a medicament for treating "the Disorders".

The present invention also provides a pharmaceutical composition for use in the treatment of "the disorders" which comprises a controlled release oral dosage form containing compound X, its parent free base or any other pharmaceutically acceptable salt thereof.

The following examples illustrate the present invention.

### Examples

In the following examples, the weight shown is the weight of free base; compound X is the hydrochloride salt. (pfb = pure free base). Mesh sizes are US standard.

#### Example 1 (Wax matrix)

Compound X	0.005-0.1 mg pfb
Gelucire 62/05 (Gattefosse)	190 mg
Propylene glycol	10 mg

#### Example 2 (Film coated pellets)

Component	mg/capsule (500 mg)	Function
Compound X	0.005-0.1 mg pfb	Active
Lactose	300	Hydrophilic diluent
Avicel PH 101 (FMC)	200	Inert pellet matrix
Film coat:	w/w of pellet cores	
Surelease (Colorcon)	2 - 10%	Release controlling polymer coat
Silicone antifoam		Antifoaming agent

**Example 3 (Film coated pellets)**

<b>Component</b>	<b>mg/capsule (500 mg)</b>	<b>Function</b>
Compound X	0.005-0.1 mg pfb	Active
Lactose	400	Hydrophilic diluent
Avicel PH 101	100	Inert pellet matrix
<b>Film coat:</b>		
	w/w of pellet cores	
Aquacoat (FMC)	2 - 10%	Release controlling polymer coat
Silicone antifoam		Antifoaming agent
Di-butylsebacate	20 - 30% (of polymer weight)	Plasticizer

In Examples 2 and 3, pellets are produced by extrusion/spheronization, using water as a granulation liquid and an appropriate size fraction is obtained by screening.

5 Pellets are then coated in a fluid bed coater (bottom spray) with 2-10% (w/w) of an aqueous Surelease dispersion (15% solids in dispersion).

Desired release profiles are obtained by mixing uncoated (= immediate release pellets) and coated pellets of suitable coating levels (= sustained release pellets), that are then filled into hard gelatine capsules.

10

**Example 4 (matrix pellets)**

<b>Component</b>	<b>mg/capsule (500 mg)</b>	<b>Function</b>
Compound X	0.005-0.1 mg pfb	Active
Glyceryl behenate	200	Hydrophobic matrix
Avicel PH 101	300	Inert pellet matrix
Sodium lauryl sulphate	0.1	Wetting agent

Pellets are produced by extrusion/spheronization using water and sodium laurylsulphate as a granulation liquid, and an appropriate size fraction is obtained by screening. Pellets may additionally be coated in a fluid bed coater (bottom spray) with  
 15 aqueous polymer dispersions to further reduce release rates and obtain the desired release profiles.

**Example 5 (Hydrogel matrix)**

Excipient	% w/w	mg /tablet	mg/tablet
Compound X	0.003-0.07pfb	0.005pfb	0.1pfb
Hydroxypropylcellulose	25	37.5	37.5
Purified water	-	-	-
Starch	to 100	109.5	108.5
Magnesium stearate	2	3.0	3.0
Total	100	150	150

Tablets may be prepared by the following procedure:

1. Blend the starch and HPC in a high shear mixer
- 5 2. Dissolve the drug into a small quantity of water and spray into blend while mixing
3. Wash spray mechanism with small volume of water into blend while mixing
4. Granulate mix with sufficient water to achieve a medium to heavy granule
5. Partially dry granule
6. Screen through a suitable mill
- 10 7. Complete drying of milled granule
8. Lubricate with Mg stearate
9. Compress into tablets with a target weight of 150mg

**Example 6 (Wax matrix)**

Excipient	% w/w	mg /tablet	mg/tablet
Compound X	0.003 to 0.07pfb	0.005pfb	0.1pfb
Lactose Anhydrous	to 100	to 150	to 150
Gelucire 62/05	18	27.0	27.0
Magnesium stearate	2	3.0	3.0
Total	100	150	150

15

Tablets may be prepared by the following procedure:

1. Preblend the drug with a small quantity of lactose
2. Sandwich the drug preblend with the remaining lactose and the required % of Gelucire 62/05 in a preheated pelletiser.
- 20 3. Pelletise until the required pellet size has been achieved
4. Remove the pellets and allow them to cool
5. Screen pellets as necessary
6. Lubricate pellets
7. Compress or encapsulate pellets

**Example 7 (Controlled release bilayer tablet)****Active Layer**

	<b>Component</b>	<b>mg/tablet</b>	<b>Function</b>
	Compound X	0.005-0.1mg pfb	Active
5	Hydroxypropylmethylcellulose	68.5	Hydrogel matrix former
	Mannitol	20	Soluble filler
	Ethyl cellulose (applied in ethanolic solution)	7.5	Binder
	Magnesium stearate	2	Lubricant
10	Colloidol silica	2	Glidant

**Support platform**

	<b>Component</b>	<b>mg/tablet</b>	<b>Function</b>
15	Hydroxypropylmethylcellulose	39.75	Hydrogel matrix former
	Hydrogenated castor oil	6.5	Insoluble filler
	Ethylcellulose (applied in ethanolic solution)	2.5	Binder
	Yellow iron oxide pigment	0.5	Pigment
	Magnesium stearate	0.5	Lubricant
20	Colloidal silica	0.25	Glidant

Tablets may be prepared as described in US5433123.

**Example 8 (Wax matrix)**

	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
25	Compound X	0.02pfb	Active
	Gelucire 50/02	91.5	Wax matrix
	Gelucire 50/13	5	Wax matrix
	Propylene glycol	1.98	Solvent
	Colloidal silica	1.5	Hydrophobic excipient
30	Sodium dihydrogen citrate	0-1.5	Stabilizer

**Process:**

The Gelucire waxes were melted together at around 60 degrees C. Compound X was dissolved in propylene glycol, and blended into the waxes. The colloidal silica was then also blended in, and the mixture filled into size 3 hard gelatin capsule shells.

Table 1.: Release Profile of wax-filled capsules of Compound X in water (0% citrate)

Time (hr):	% Released
1	13
3	29
5	53
8	73

**Example 9 (Ethylcellulose coated beads)**

- 5 200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:

Component	% w/w	Function
Compound X	0.003-0.05pfb	Active
10 Opadry® Clear	3	Binder
Sodium dihydrogen citrate	1.5	Stabilizer
Purified water	q.s.	
Total	100	

- 15 Seal coating solution: A solution of Opadry® Clear (YS-1-9025A) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900 grams of purified water.

- Polymer Coating: A polymer coating dispersion containing ethylcellulose  
 20 (Surelease®) of the following composition was made and used for polymer coating the seal coated beads at an 10% to 25% weight gain, in particular 10, 12, 15, 17, 22 and 25%.

Component	% w/w	Function
25 Surelease®	60 (25% as solids)	Release controlling polymer coat with plasticiser
Purified water	q.s.	
Total	100	

- 30 Drug layered beads were produced by layering the drug solution onto 25-30 mesh non-pareil beads using a Niro STREA-1 fluid bed dryer so as to layer 100 micrograms of the drug as the free base onto 200 mg of the non-pareil beads. The drug layered beads were seal coated with Opadry® Clear seal coating solution to a weight gain of 3% to produce

the immediate release beads. A portion of the immediate release beads were polymer coated to a weight gain of 10% to 25% with the Surelease® coating dispersion. The final polymer coated beads were produced by seal coating the polymer coated beads to a weight gain of 2% with the Opadry® Clear seal coating solution.

5

Table 2. Release Profile Range of Ethylcellulose coated beads, 10-25% by weight of Compound X in Water

Time (hr)	% Released
1	0.8-36
2	5-57
4	13-75
8	18-91

10 **Example 10 (Ethylcellulose coated beads)**

200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:

Component	% w/w	Function
15 Compound X	0.003-0.05pfb	Active
Opadry® Clear	3	Binder
Sodium dihydrogen citrate	1.5	Stabilizer
Purified water	q.s.	
Total	100	

20

Seal coating: A seal coating dispersion containing Eudragit® L30D-55 of the following composition was made and used for seal coating the drug layered beads at an 4% weight gain.

Component	% w/w	Function
25 Eudragit® L30D-55	45 (30% as solids)	Polymeric seal coat
Triethyl citrate	2.02	Plasticizer
Talc	3.10	Anti-tack
Purified water	q.s.	
30 Total	100	

Polymer Coating: A polymer coating dispersion containing ethylcellulose (Surelease®) of the following composition was made and used for polymer coating the seal coated beads at an 10% to 25% weight gain.

5	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
	Surelease®	60 (25% as solids)	Release controlling polymer coat with plasticiser
	Purified water	q.s.	
	Total	100	

10

Drug layered beads were produced by layering the drug solution onto 25-30 mesh non-pareil beads using a Niro STREA-1 fluid bed dryer so as to layer 100 micrograms of the drug as the free base onto 200 mg of the non-pareil beads. The drug layered beads were seal coated with Eudragit® L30D-55 seal coating dispersion to a weight gain of 4% to produce the immediate release beads. A portion of the immediate release beads were polymer coated to a weight gain of 10% tp 25% with the Surelease® coating dispersion. The final polymer coated beads were produced by seal coating the polymer coated beads to a weight gain of 2% with the Opadry® Clear seal coating solution.

20

Table 3: Release Profile of Eudragit® L30D Seal Coated/Ethylcellulose Coated Beads of Compound X in Water

Time (hr)	% Released, 10% Surelease
0.5	1.5
1	5
2	20
4	39
6	49
8	56

25

**Example 11 (Ethylcellulose coated beads)**

200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:



Component	% w/w	Function
Compound X	0.003-0.05pfb	Active
Opadry® Clear	3	Binder
Sodium dihydrogen citrate	1.5	Stabilizer
5 Purified water	q.s.	
Total	100	

Seal coating solution: A solution of Opadry® Clear (YS-1-9025A) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900  
10 grams of purified water.

Polymer Coating: A polymer coating dispersion containing Ethylcellulose (Aquacoat®) of the following composition was made and used for polymer coating the seal coated beads at a 10% weight gain.

Component	% w/w	Function
Aquacoat®	50 (30% as solids)	Release controlling polymer coat
Triethyl Citrate	2.02	Plasticizer
Purified water	q.s.	
20 Total	100	

Drug layered beads were produced by layering the drug solution onto 25-30 mesh non-pareil beads using a Niro STREA-1 fluid bed dryer so as to layer 100 micrograms of the drug as the free base onto 200 mg of the non-pareil beads. The drug layered beads were  
25 seal coated with Opadry® Clear seal coating solution to a weight gain of 3% to produce the immediate release beads. A portion of the immediate release beads were polymer coated to a weight gain of 10% with the Aquacoat® coating dispersion. The final polymer coated beads were produced by seal coating the polymer coated beads to a weight gain of 2% with the Opadry® Clear seal coating solution.

30

#### Example 12 (Eudragit coated beads)

200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:

	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
	Compound X	0.003-0.05pfb	Active
	Opadry® Clear	3	Binder
	Sodium dihydrogen citrate	1.5	Stabilizer
5	Purified water	q.s.	
	Total	100	

Seal coating solution: A solution of Opadry® Clear (YS-1-9025A) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900 grams of purified water.

Polymer Coating: A polymer coating dispersion containing Eudragit® RS or RS/RL of the following composition was made and used for polymer coating the seal coated beads at an 10% weight gain.

	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
	Eudragit® RS 30D	45 (30% as solids)	Release controlling polymer coat
	Triethyl citrate	2.02	Plasticizer
	Talc	3.10	Anti-tack
20	Purified water	q.s.	
	Total	100	

or

	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
25	Eudragit® RS 30D	36 (30% as solids)	Release controlling polymer coat
	Eudragit® RL 30D	9 (30% as solids)	Release controlling polymer coat
	Triethyl citrate	2.02	Plasticizer
	Talc	3.10	Anti-tack
30	Purified water	q.s.	
	Total	100	

Drug layered beads were produced by layering the drug solution onto 25-30 mesh non-pareil beads using a Niro STREA-1 fluid bed dryer so as to layer 100 micrograms of the drug as the free base onto 200 mg of the non-pareil beads. The drug layered beads were seal coated with Opadry® Clear seal coating solution to a weight gain of 3% to produce the immediate release beads. A portion of the immediate release beads were polymer

coated to a weight gain of 10% with the Eudragit® RS or RS/RL coating dispersion. The final polymer coated beads can be produced by seal coating the polymer coated beads to a weight gain of 2% with the Opadry® Clear seal coating solution.

5 Table 4: Release Profile of Eudragit® RS/RL coated beads of Compound X in water

Time (hr)	% Released
0.5	0.2
1	0.3
2	0.4
4	1.9
6	13
8	20

**Example 13 (Methocel coated beads)**

10 200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:

Component	% w/w	Function
Compound X	0.003-0.05pfb	Active
15 Methocel E4M	15	Release controlling polymer coat
Sodium dihydrogen citrate	1.5	Stabilizer
Purified water	q.s.	
Total	100	

20 Seal coating solution: A solution of Opadry® Clear (YS-1-7006) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900 grams of purified water.

**Example 14 (Ethylcellulose coated beads with a retardant)**

25 200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:

	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
	Compound X	0.003-0.05pfb	Active
	Opadry® Clear	1.5	Binder
	Surelease®	1.5	Retardant
5	Sodium dihydrogen citrate	1.5	Stabilizer
	Purified water	q.s.	
	Total	100	

10 Seal coating solution: A solution of Opadry® Clear (YS-1-9025A) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900 grams of purified water.

15 Polymer Coating: A polymer coating dispersion containing Ethylcellulose (Surelease®) of the following composition was made and used for polymer coating the seal coated beads at 10% weight gain.

	<b>Component</b>	<b>% w/w</b>	<b>Function</b>
	Surelease®	60 (25% as solids)	Release controlling polymer coat with plasticiser
20	Purified water	q.s.	
	Total	100	

25 Drug layered beads were produced by layering the drug solution onto 25-30 mesh non-pareil beads using a Niro STREA-1 fluid bed dryer so as to layer 100 micrograms of the drug as the free base onto 200 mg of the non-pareil beads. The drug layered beads were seal coated with Opadry® Clear seal coating solution to a weight gain of 3% to produce the immediate release beads. A portion of the immediate release beads were polymer coated to a weight gain of 10% with the Surelease® coating dispersion. The final polymer coated beads can be produced by seal coating the polymer coated beads to a  
30 weight gain of 2% with the Opadry® Clear seal coating solution.

Table 5. Release Profile of Ethylcellulose Coated Beads,  
with Retardant, of Compound X in Water

Time (hr)	% Released	
	Without Retardant	With Retardant
0.5	12	8
1	37	22
2	57	35
4	73	48
6	85	53
8		58

5 **Example 15 (Enteric coated beads)**

200 mg of non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size may be used. A medicated layer solution of the following composition was used:

	Component	% w/w	Function
10	Compound X	0.003-0.05pfb	Active
	Opadry® Clear	3	Binder
	Sodium dihydrogen citrate	1.5	Stabilizer
	Purified water	q.s.	
	Total	100	

15

Seal coating solution: A solution of Opadry® Clear (YS-1-9025A) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900 grams of purified water.

20 **Polymer Coating:** A polymer coating dispersion containing Eudragit® L30D-55 of the following composition was made and used for polymer coating the seal coated beads at an 20% weight gain.

	Component	% w/w	Function
25	Eudragit L30D-55	45.00 (30% as solids)	Enteric (pH dependent) polymer
	Triethyl citrate	2.02	Plasticizer
	Talc	3.10	Anti-tack
	Purified water	q.s.	
	Total	100	

Drug layered beads were produced by layering the drug solution onto 25-30 mesh non-pareil beads using a Niro STREA-1 fluid bed dryer so as to layer 100 micrograms of the drug as the free base onto 200 mg of the non-pareil beads. The drug layered beads were seal coated with Opadry® Clear seal coating solution to a weight gain of 3% to produce the immediate release beads. A portion of the immediate release beads were enteric coated to a weight gain of 20% with the Eudragit® enteric coating dispersion. The final enteric coated beads were produced by seal coating the enteric coated beads to a weight gain of 2% with the Opadry Clear seal coating solution.

10

**Example 16 (matrix tablet)**

Ingredient	mg/tablet	Function
Compound X	0.005-0.1pfb	Active
Hydroxypropyl Methcellulose E4M CR	.75.0	Hydrogel matrix
15 Sodium Dihydrogen Citrate	3.00	Stabilizer
Lactose, Fast Flo	70.38	Hydrophilic diluent
Magnesium Stearate	1.50	Lubricant
Opadry® White	2.25	Seal coat polymer

20 Seal coating solution: A solution of Opadry® Clear (YS-1-9025A) in purified water at 10% solids concentrations was made by dissolving 100 grams of Opadry® Clear into 900 grams of purified water.

25 Polymer Coating: A polymer coating dispersion containing Ethylcellulose (Surelease®) of the following composition was made and used for polymer coating the seal coated beads at 10% weight gain.

Component	% w/w	Function
30 Surelease®	60 (25% as solids)	Release controlling polymer coat with plasticiser
Purified water	q.s.	
Total	100	

35 700 grams of core tablets were coated using a Vector LDCS pan to a 3% weight gain with the Opadry® Clear seal coating solution. The seal coated tablets were then polymer coated to 4% weight gain using the Surelease® coating dispersion.

Table 6. Release Profile for a Matrix Tablet of Compound X in water

Time (hr)	% Dissolved
1	8
2	30
4	58
8	96

5 **Example 17 (Controlled release bilayer tablet)****Active Layer**

	Component	mg/tablet	Function
	Compound X	0.005-0.1 mg pfb	Active
	Methocel K4M	15.00	Hydrogel polymer
10	Lactose monohydrate	62.0	Hydrophilic filler
	Polyvinylpyrrolidone	3.0	Binder
	Magnesium stearate	1.0	Hydrophobic lubricant
	Syloid 244	1.0	Hydrophilic glidant

15 **Support platform**

	Component	mg/tablet	Function
	Compritol 888	15.0	Plasticizer
	Lactose monohydrate	29.0	Hydrophilic filler
20	Polyvinylpyrrolidone	4.0	Binder
	Magnesium stearate	1.5	Hydrophobic lubricant
	Methocel E5	29.4	Hydrogel polymer
	Iron oxide	0.1	Colourant

CLAIMS

1. A controlled release oral dosage form containing [R-(Z)]- $\alpha$ -(methoxyimino)- $\alpha$ -(1-azabicyclo [2.2.2]oct-3-yl)acetonitrile monohydrochloride (compound X), its parent free base or any other pharmaceutically acceptable salt thereof.
  - 5 2. A dosage form according to claim 1 which provides an *in vitro* release profile selected to provide an area under the *in vivo* plasma profile curve that is similar to that obtained following conventional oral administration of a fast release tablet 5 to 75 $\mu$ g (calculated as free base) compound X twice a day.
  - 3 A dosage form according to claim 1 or 2 which provides an *in vitro* release profile  
10 of 25-70% over 4 hours and 70-100% over 8 hours.
  4. A dosage form according to any of claims 1 to 3 selected from wax matrices, swellable and/or gellable matrices, tablets coated with release controlling polymers or waxes, and pellets, granules or beads comprising matrices or coated with release  
15 controlling polymers or waxes and then formulated as capsules, compressed tablets or suspensions.
  5. A dosage form according to any preceding claim comprising a swellable and/or gellable matrix selected from alkyl celluloses, hydroxyalkylcelluloses, polyvinyl alcohol, polymethacrylates, polymethylmethacrylates, methacrylate/divinylbenzene copolymers, carboxymethylamide, polyoxyalkylene glycols, polyvinyl pyrrolidone and carboxymethyl  
20 cellulose.
  6. A dosage form according to claim 5 wherein the matrix is selected from alkyl celluloses, hydroxyalkylcelluloses, polyvinyl alcohol, polymethacrylates, cross-linked polyvinylpyrrolidone and sodium carboxymethyl cellulose.
  7. A dosage form according to claim 5 or 6 comprising a hydrogel matrix tablet  
25 coated with a hydrophobic release controlling polymer coating selected from alkyl celluloses and methacrylic acid derivatives.
  8. A dosage form according to claim 7 wherein the polymer matrix comprises 10-50% and the hydrophobic release controlling polymer comprises 4-10% by weight of the tablet.
  - 30 9. A dosage form according to claim 7 or 8 comprising a tablet of the following composition (mg/tablet):
- |                                    |              |
|------------------------------------|--------------|
| Compound X                         | 0.005-0.1pfb |
| Hydroxypropyl Methcellulose E4M CR | 75.0         |
| Sodium Dihydrogen Citrate          | 0-3.00       |
| 35 Lactose, Fast Flo               | 70.38-73.38  |
| Magnesium Stearate                 | 1.50         |
| Opadry® White                      | 2.25         |



- seal coated with a solution of Opadry® Clear (YS-1-7006) in purified water at 10% solids concentrations and polymer coated with a 60% w/w (25% as solids) dispersion containing Ethylcellulose (Surelease®) at 10% weight gain, formed into core tablets, coated with the Opadry® Clear seal coating solution and polymer coated to 4% weight gain using 60% w/w (25% as solids) dispersion containing Ethylcellulose (Surelease®). -
- 5 10. A dosage form according to any of claims 1 to 4 which comprises drug-layered beads coated with a release controlling polymer either alone or in combination with drug-layered beads not coated with a release controlling polymer (immediate release beads) and optionally, inert excipients and/or retardants and/or one or more binders.
- 10 11. A dosage form according to claim 10 wherein the layered beads are seal coated with a film-forming polymer.
12. A dosage form according to claim 10 or 11 wherein the release controlling polymer coating is selected from from alkyl celluloses, hydroxyalkylcelluloses, sodium carboxymethyl cellulose and methacrylic acid derivatives.
- 15 13. A dosage form according to any of claims 10 to 12 wherein the polymer(s) make up 10 to 30% by weight of the total dosage form.
14. A dosage form according to claim 10 in capsule form comprising non-pareil sugar beads of 16-20, 20-25 or 25-30 mesh size, coated to a drug loading of 100microgrammes (calculated as free base) per 200mg beads, with a medicated aqueous layer solution of the
- 20 following composition (%w/w):
- |                          |               |
|--------------------------|---------------|
| Compound X               | 0.003-0.06pfb |
| Opadry® Clear            | 3             |
| Sodium dihydride citrate | 0-1.5         |
- seal coated with a solution of Opadry® Clear (YS-1-7006) in purified water at 10% solids concentrations to a weight gain of 3%, and a portion of the beads further polymer coated to a weight gain of 10-25% with a 60%w/w (25% as solids) dispersion containing ethylcellulose (Surelease®) and then seal coated to a weight gain of 2% with the above seal coat.
- 25 15. A method of treatment and/or prophylaxis of dementia, including Alzheimer's disease, in mammals by administering an effective amount of a controlled release oral dosage form according to claim 1, to a sufferer in need thereof.
- 30 16. A method for enhancing amyloid precursor protein processing along a non-amyloidogenic pathway in patients suffering from, or at risk of developing, Alzheimer's disease by administering an effective amount of a controlled release oral dosage form
- 35 according to claim 1, to a sufferer in need thereof.

17. The use of a controlled release oral dosage form according to claim 1, in the manufacture of a medicament for treatment and/or prophylaxis of dementia, including Alzheimer's disease, in mammals.
18. The use of a controlled release oral dosage form according to claim 1, in the manufacture of a medicament for enhancing amyloid precursor protein processing along a non-amyloidogenic pathway in patients suffering from, or at risk of developing, Alzheimer's disease.
19. A pharmaceutical composition for treatment and/or prophylaxis of dementia, including Alzheimer's disease, in mammals which comprises a controlled release oral dosage form according to claim 1.
20. A pharmaceutical composition for enhancing amyloid precursor protein processing along a non-amyloidogenic pathway in patients suffering from, or at risk of developing, Alzheimer's disease which comprises a controlled release oral dosage form according to claim 1.
21. A dosage form, method, use or composition according to any preceding claim in which release in the gastro-intestinal tract takes place predominantly over the first eight to twelve hours following ingestion.
22. A dosage form, method, use or composition according to any preceding claim containing [R-(Z)]- $\alpha$ -(methoxyimino)- $\alpha$ -(1-azabicyclo [2.2.2]oct-3-yl)acetonitrile monohydrochloride.
23. A dosage form, method, use or composition according to any of claims 1 to 22 containing 5 $\mu$ g compound X (calculated as free base).
24. A dosage form, method, use or composition according to any of claims 1 to 22 containing 12.5 $\mu$ g compound X (calculated as free base).
25. A dosage form, method, use or composition according to any of claims 1 to 22 containing 25 $\mu$ g compound X (calculated as free base).
26. A dosage form, method, use or composition according to any of claims 1 to 22 containing 50 $\mu$ g compound X (calculated as free base).
27. A dosage form, method, use or composition according to any of claims 1 to 22 containing 75 $\mu$ g compound X (calculated as free base).
28. A dosage form, method, use or composition according to any of claims 1 to 22 containing 100 $\mu$ g compound X (calculated as free base).



## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification <sup>6</sup> : <b>A61K 31/435</b>	<b>A3</b>	(11) International Publication Number: <b>WO 98/10762</b> (43) International Publication Date: 19 March 1998 (19.03.98)
<p>(21) International Application Number: PCT/GB97/02418</p> <p>(22) International Filing Date: 8 September 1997 (08.09.97)</p> <p>(30) Priority Data: 9619074.9 12 September 1996 (12.09.96) GB</p> <p>(71) Applicants (for all designated States except US): SMITHKLINE BEECHAM PLC [GB/GB]; New Horizons Court, Brentford, Middlesex TW8 9EP (GB). SMITHKLINE BEECHAM CORPORATION [US/US]; One Franklin Plaza, P.O. Box 7929, Philadelphia, PA 19103 (US).</p> <p>(72) Inventors; and (75) Inventors/Applicants (for US only): MILOSOVICH, Susan, Marie [US/US]; SmithKline Beecham Pharmaceuticals, 1250 South Collegeville Road, P.O. Box 5089, Collegeville, PA 19426-0989 (US). MULDOON, William [US/US]; SmithKline Beecham Pharmaceuticals, 1250 South Collegeville Road, P.O. Box 5089, Collegeville, PA 19426-0989 (US). NAPPER, James, Albert [GB/GB]; SmithKline Beecham Pharmaceuticals, New Frontiers Science Park South, Third Avenue, Harlow, Essex CM19 5AW (GB). ROUSSEAU, Laurence [GB/GB]; SmithKline Beecham Pharmaceuticals, New Frontiers Science Park South, Third Avenue, Harlow, Essex CM19 5AW (GB).</p>	<p>SAUER, Joseph [US/US]; SmithKline Beecham Pharmaceuticals, 1250 South Collegeville Road, P.O. Box 5089, Collegeville, PA 19426-0989 (US).</p> <p>(74) Agent: VALENTINE, Jill, Barbara; SmithKline Beecham plc, Corporate Intellectual Property, Two New Horizons Court, Brentford, Middlesex TW8 9EP (GB).</p> <p>(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, GH, HU, ID, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, US, UZ, VN, YU, ZW, ARIPO patent (GH, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).</p> <p><b>Published</b> <i>With international search report.</i> <i>Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i></p> <p>(88) Date of publication of the international search report: 4 June 1998 (04.06.98)</p>	
<p>(54) Title: CONTROLLED RELEASE DOSAGE FORM OF R-(Z)-ALPHA-METHOXYIMINO-ALPHA-(1-AZABICYCLO2.2OCT-C- YL)ACETONITRILE MONOHYDROCHLORIDE</p> <p>(57) Abstract</p> <p>A controlled release formulation of an acetonitrile compound and its use in the treatment and/or prophylaxis of certain disorders.</p>		

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# INTERNATIONAL SEARCH REPORT

International Application No  
PCT/GB 97/02418

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 6 A61K31/435

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**  
Minimum documentation searched (classification system followed by classification symbols)  
IPC 6 A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT		Relevant to claim No.
Category	Citation of document, with indication, where appropriate, of the relevant passages	
X	WO 95 31457 A (SMITHKLINE BEECHAM PLC ;KEOGH JOHN (GB); BORRETT GARY THOMAS (GB);) 23 November 1995 see page 8, line 31 - line 36 ---	1-7, 15, 17, 19-22
X	WO 96 12486 A (SMITHKLINE BEECHAM PLC ;MARKWELL ROGER EDWARD (GB); HAWKINS JULIE) 2 May 1996 cited in the application see page 2, line 11 - line 23 ---	1-7, 15-23
X	EP 0 392 803 A (BEECHAM GROUP PLC) 17 October 1990 cited in the application see page 10, line 39 - line 43 ---	1-7, 15, 17, 19-22
	-/--	

<input checked="" type="checkbox"/> Further documents are listed in the continuation of box C.	<input checked="" type="checkbox"/> Patent family members are listed in annex.
<p>° Special categories of cited documents :</p> <p>*A* document defining the general state of the art which is not considered to be of particular relevance</p> <p>*E* earlier document but published on or after the international filing date</p> <p>*L* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>*O* document referring to an oral disclosure, use, exhibition or other means</p> <p>*P* document published prior to the international filing date but later than the priority date claimed</p>	
<p>*T* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>*X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone</p> <p>*Y* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>*g* document member of the same patent family</p>	
Date of the actual completion of the international search  24 March 1998	Date of mailing of the international search report  24. 04. 98
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tx. 31 651 epo nl, Fax: (+31-70) 340-3016	Authorized officer  Boulois, D

# INTERNATIONAL SEARCH REPORT

International Application No  
PCT/GB 97/02418

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
P,X	WO 97 04750 A (SMITHKLINE BEECHAM PLC ;NAPPER JAMES ALBERT (GB); MORTIMER NEIL (G) 13 February 1997 see page 3, line 21 - line 24 -----	1-7,15, 17,19-22

Form PCT/ISA/210 (continuation of second sheet) (July 1992)

1

# INTERNATIONAL SEARCH REPORT

International application No.  
PCT/GB 97/02418

## Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1.  Claims Nos.:  
because they relate to subject matter not required to be searched by this Authority, namely:  
see FURTHER INFORMATION sheet PCT/ISA/210
2.  Claims Nos.:  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3.  Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1.  As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2.  As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3.  As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4.  No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

### Remark on Protest

- The additional search fees were accompanied by the applicant's protest.
- No protest accompanied the payment of additional search fees.

Form PCT/ISA/210 (continuation of first sheet (1)) (July 1992)

**INTERNATIONAL SEARCH REPORT**

International Application No. PCT/GB 97/02418

**FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210**

Remark : Although claims 15, 16, 21-28 are directed to a method of treatment of the human/animal body , the search has been carried out and based on the alleged effects of the compound/composition.



# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/GB 97/02418

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